GE's "Revolution CT"



MATLAB III: CT

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https://www.zmescience.com/medicine/inside-human-body-real-time-gifs-demo-power-ct-scan/

Reminders

- Make sure you have MATLAB and the toolboxes (Signal Processing, Image Processing) installed
- Download the zip file from LMS and extract all files into your MATLAB folder

Theory of CT

General theory of CT

- X-ray projections are taken at multiple views Attenuation due to different properties of tissue
- Solve the inverse problem to get tomographic information (CT = computed tomography)



2D projection

3D imaging

Resolution of CT reconstruction

- Number of rays affects the radial component of spatial resolution
- Number of views affects the circumferential component of resolution



Radon transform

- Representation of the X-ray projection data in the form of a sinogram
- Indicates characteristics of the sample
 - Objects closer to the field of view produce a high amplitude in the sinogram

 $F(\theta, s) = = \int_{-\infty}^{+\infty} f(s\cos\theta + t\sin\theta, -t\cos\theta + s\sin\theta)dt$





Inverse radon transform: Fourier slice theorem

- 1D Fourier Transform (FT) of the RT projection profile acquired at angle φ is equivalent to the value of the 2D FT of f(x,y) along a line at the inclination angle φ
- Putting together RT profiles at all acquisition angles yields the full 2D FT
- Image can be reconstructed using the inverse 2D FT



Back-projection

- Standard method of reconstructing CT slices
- Sinogram is used to back-project each view, then all views are combined to get the whole image



Filtered back-projection (FBP)

- Unfiltered back-projection from a normal sinogram can produce a blurry image
 - A filter is required in the sinogram space







FBP in progress



How can we use MATLAB for CT? 1. Parallel beam CT 2. Fan beam CT







Parallel beam CT

Parallel beam: *radon*

- Beams (1 pixel apart) from the source are projected parallel to the detector and sample
- Parallel beams and detector are rotated around the center of the image at an angle theta $\boldsymbol{\theta}$



[R, xp] = radon(I, theta);

R = value
xp = detector locations
I = input image
theta = rotation angle

Change p_type (Line 5) to 1, 2, or 3 for different sample types Example 1: Parallel beam

• Run Ex1_parallel.m

Image domain

• As θ (red arrow) is changing, information is added to the sinogram!





Sinogram domain

Example 1: Parallel beam

What happens when we change the θ step (Line 23) to 5? What is happening here?



Collected angles are more discrete (fewer angular views, lower resolution)

 $\mathsf{R}_{\theta}(\mathsf{X}')$

Example 1: Parallel beam

What happens if you change the max θ (Line 22) to 45? What is happening here?



Parallel beam back-projection: iradon

- Back-projection for parallel beam sinograms
- Filtered back-projection can be implemented

I = iradon(R, theta, *interp, filter*);

I = reconstructed image R = sinogram theta = rotation angle interp = interpolation method filter = filter to be used for FBP (interp, filter are optional)

Change p_type (Line 5) to 1, 2, or 3 for different sample types Example 2: Parallel beam BP

- Run Ex2_parallel_back.m
- Line 32 implements normal BP (no filter)
- Line 35 implements filtered BP
 - 'Hamming' can be replaced with other filter types
 - 'Ram-Lak'
 - 'Shepp-Logan'
 - 'Cosine'
 - 'Hann'



filtered backprojected image



Example 2: Parallel beam BP

 What happens if you change the maximum θ (Line 23) or step (Line 24)?



Fan beam CT

Fan beam: *fanbeam*

- Source beams are projected in a fan shape from a beam vertex
- D is the distance between the fan beam vertex and sample's center of rotation
- Source and detector are rotated at an angle $\boldsymbol{\theta}$



Fan beam: *fanbeam*

- Calculates projection data for a specified fan beam geometry
- Rotation angles (θ) fixed at 0 to 360 degrees

[F1, sensor_pos1, fan_rot_angles1] = fanbeam(P, D, 'FanSensorSpacing', dsensor1);

> F1 = output sensor_pos1 = sensor positions fan_rot_angles1 = fan rotation angles P = input image D= distance to object FanSensorSpacing = specific property dsensor1 = spacing between sensors (FanSensorSpacing, dsensor1 are optional)

Fan beam FBP: *ifanbeam*

- Converts the fan-beam data to parallel beam projections
- Uses the filtered back projection algorithm to perform the inverse Radon transform
- Ifan1 = ifanbeam(F1, D, 'FanSensorSpacing', dsensor1);

Ifan1 = output
F1 = sinogram
D= distance to object
FanSensorSpacing = specific property
dsensor1 = spacing between sensors
(FanSensorSpacing, dsensor1 are optional)

Change p_type (Line 5) to 1, 2, or 3 for different sample types Example 3: fan beam CT

- Run Ex3_fanbeam.m
- D (Line 25) is slightly larger than half the diagonal distance of image (convention),
- Dsensor = 1 (Line 26)







Example 3: fan beam CT

 What happens if you change the sensor spacing (Line 26) from 1 to 5? From 1 to 0.5? (D unchanged)









The resolution is related to the sensor spacing (high spacing = low resolution)

Example 3: fan beam CT

What happens if you increase D in Line 28?
 (Dsensor = 1)

28 - [F, pos, theta] = fanbeam(img, D'FanSensorSpacing', Dsensor);







D = default (~191)

D = 300

Higher source-object distance gives lower reconstruction resolution **D** = 500

BB13 Homework

Read the web page carefully and run the codes on your PC: http://www.mathworks.com/help/images/radon-

transform.html?refresh=true

Then write a similar page with an ellipse as your object (instead of the square).

Use the iradon function to reconstruct your ellipse.

Due Date: Tuesday 3/20 (11:59PM)

BB14 Homework

Green Book 1.14, 1.15 and 1.18



Optional:

As an Art_X Project, Please Design Portable CT Scanner in an Auto-driving Car, or a CT Scanner for a Novel Application.

Due Date: Friday 3/23 (11:59PM)

https://arxiv.org/ftp/arxiv/papers/1312/1312.6046.pdf http://content.iospress.com/articles/journal-of-x-ray-science-and-technology/xst00453 Thank you